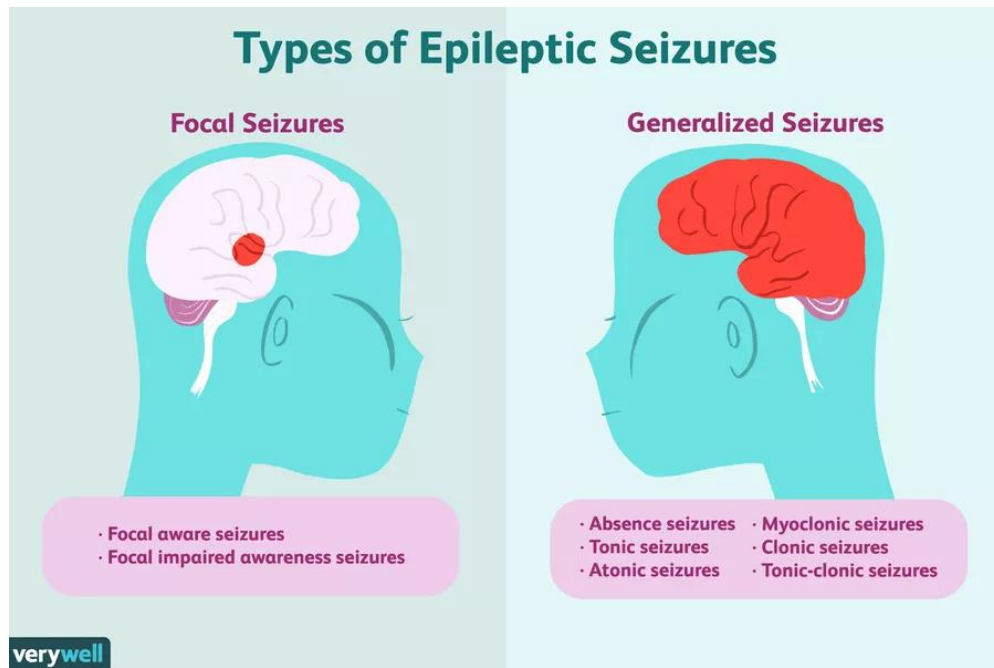
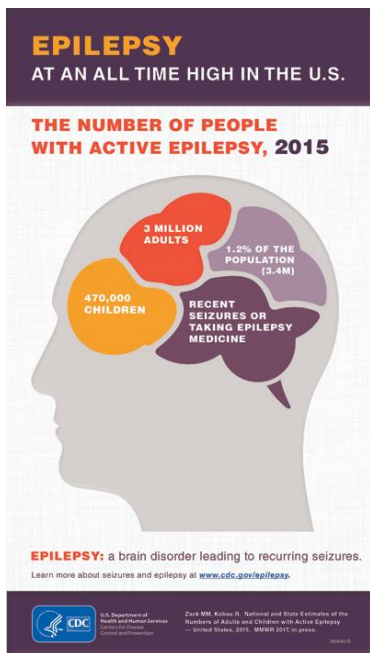


A deep learning-based method for automatic detection of epileptic seizure in a dataset with both generalized and focal seizure types

Authors:

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A general seizure detection outline

EEG signal recording

Preprocessing (ICA, segmentation of entire epochs, etc.)

Automatic or Hand-engineered feature extraction

Seizure detection using some Machine Learning method

Performance metrics of the previous studies on Seizure detection

Related works	Method	Accuracy	Sensitivity	Specificity	Precision	F-measure	Dataset
Vidyarante et al.	DRNN on raw EEG data	–	100	99.2	–	–	CHB-MIT
Birjandtalab et al.	Normalized Spectral features + MLP for each subject	–	96.27	–	94.21	95.3	21 patients
Bolagh et al.	Subject-selection and Subject-clustering to select relevant individuals	89.84	85.87	89.64	–	–	CHB-MIT
Talha Avcu et al.	SeizNet, a CNN for seizure detection	–	95.8	–	–	–	29 patients

public datasets used in the literature of the seizure detection

Name of dataset	# subjects	recording	Types of seizure
CHB-MIT [11]	22	21 channel scalp EEG	Not mentioned
Freiburg [9]	21	126 channels Intracranial electrodes	Focal
Bonn [4]	-	Intracranial electrodes, single channel	Focal
TUH [12]	ongoing	21 channel scalp EEG	Generalized and Focal

Main drawbacks of the mentioned studies on Seizure detection

Hand-engineered features

Using a dataset that consists of only one kind of seizure

Less attention to the cross-subject learning

We process raw EEG signals using a DL framework

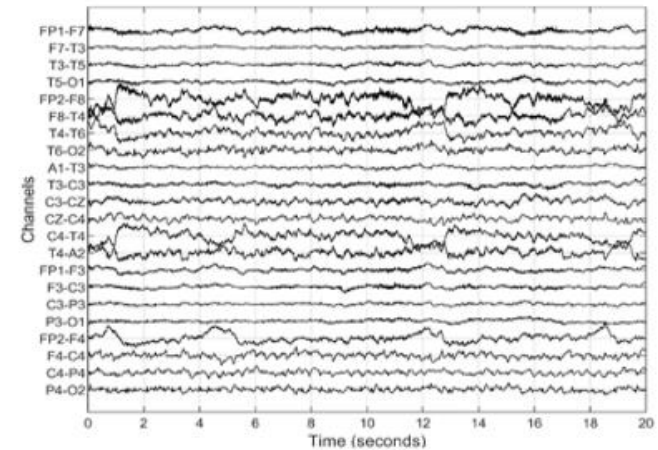
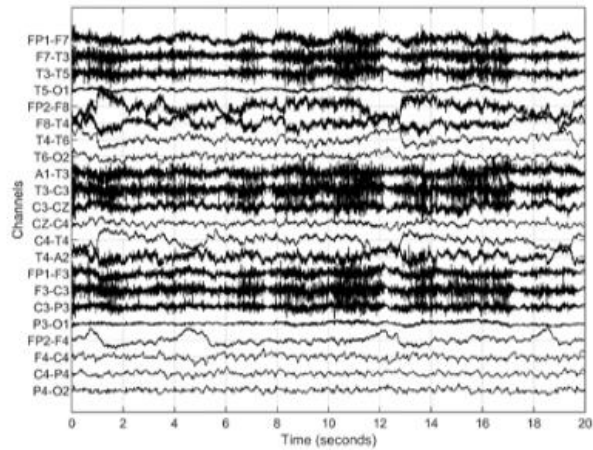
We use a dataset with both generalized and focal seizure types

We use LOSO as a cross-subject scenario

Dataset used in this paper

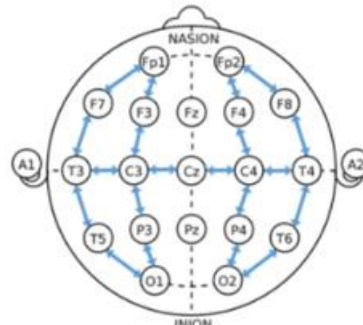
Name of dataset	# subjects	recording	Types of seizure	Sampling frequency	Length of recordings
TUH	Ongoing (>70)	21 channel scalp EEG	Generalized and Focal	250 or 256 Hz	Between 10 to 60 minutes

➤ Preprocessing scheme:ICA and CCA for
artifact reductionNotch filter to remove
base-line noiseRemoving frequencies less than
0.5 HzTransformation to TCP montage
with 22 channels



EEG signal contaminated with EMG artifacts. This artifact can be seen with high frequency (>30 Hz) activity in some channels such as FP1-F7 (patient ID 00000177).

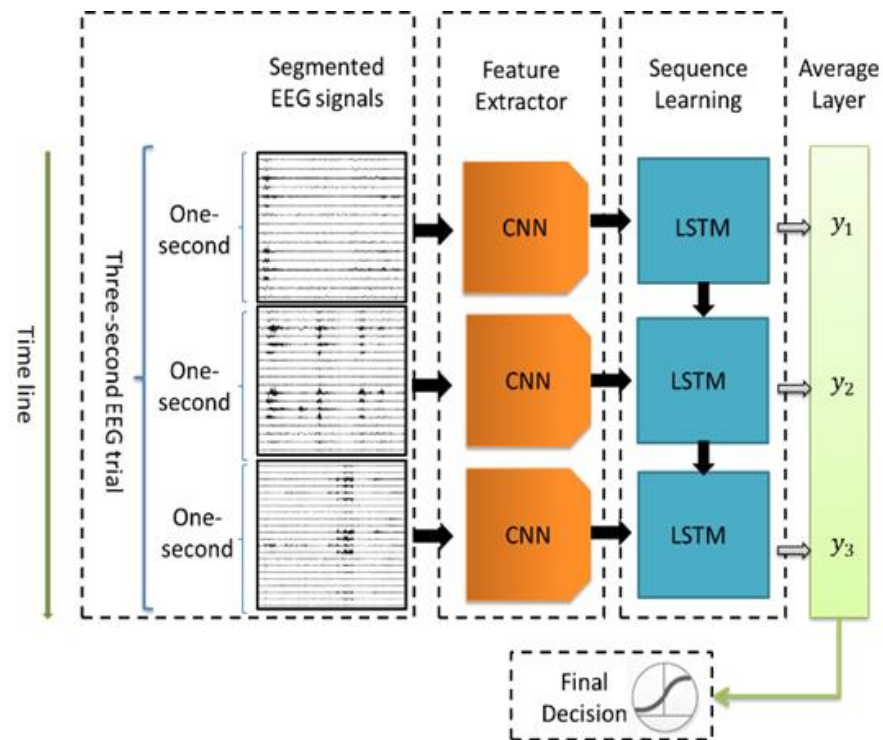
EEG signals after automatic artifact reduction. EMG artifacts in channels such as FP1-F7 are reduced using BSS method (patient ID 00000177).



- | | |
|-----------------|------------------|
| Montage0 FP1-F7 | Montage11 CZ-C4 |
| Montage1 F7-T3 | Montage12 C4-T4 |
| Montage2 T3-T5 | Montage13 T4-A2 |
| Montage3 T5-O1 | Montage14 FP1-F3 |
| Montage4 FP2-F8 | Montage15 F3-C3 |
| Montage5 F8-T4 | Montage16 C3-P3 |
| Montage6 T4-T6 | Montage17 P3-O1 |
| Montage7 T6-O2 | Montage18 FP2-F4 |
| Montage8 A1-T3 | Montage19 F4-C4 |
| Montage9 T3-C3 | Montage20 C4-P4 |
| Montage10 C3-CZ | Montage21 P4-O2 |

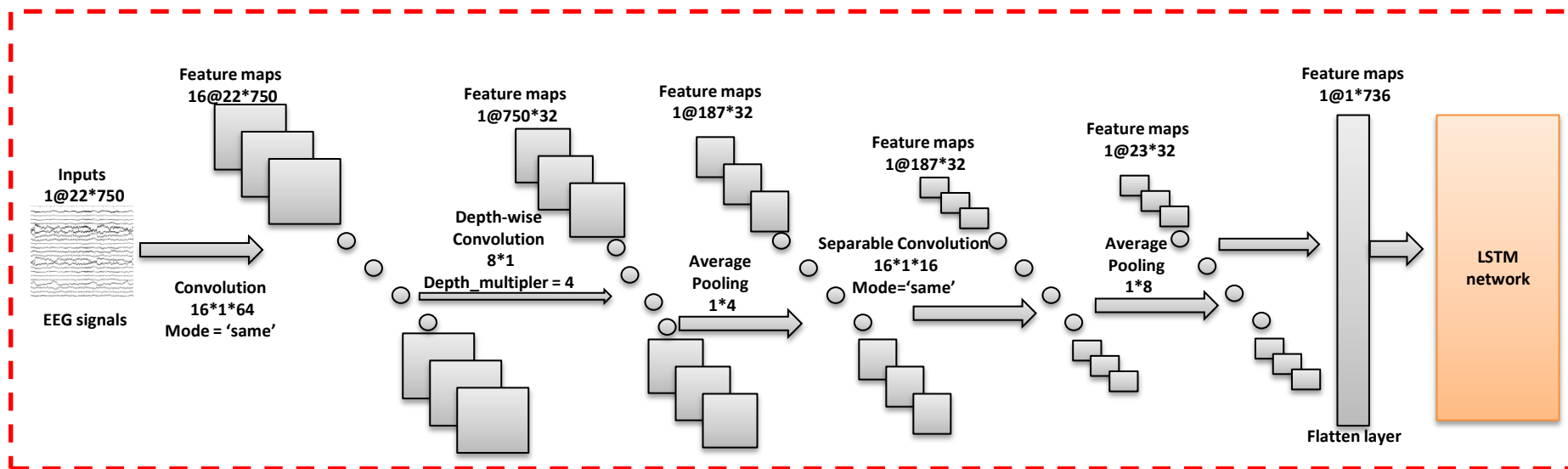
TCP or double banana montage which is used in clinical seizure detection.

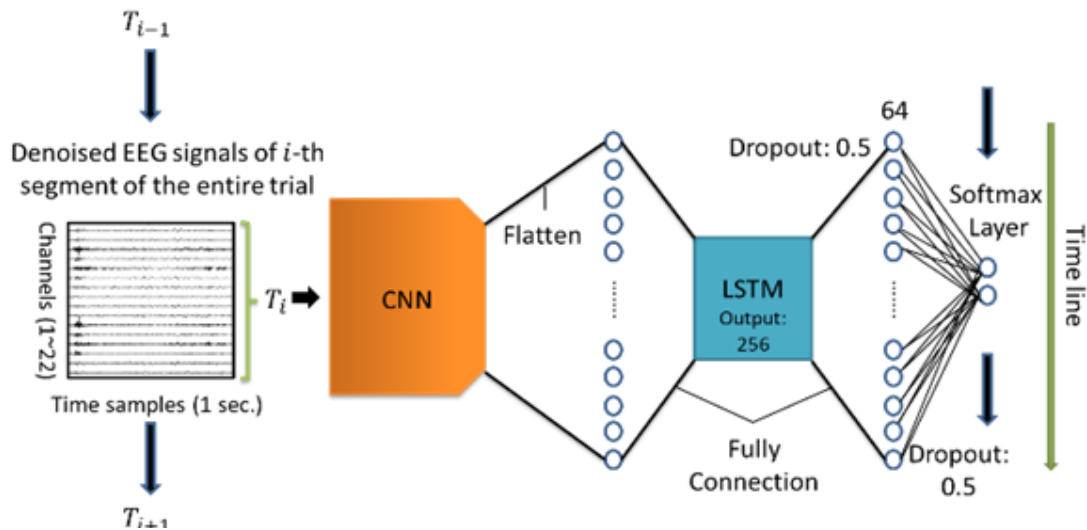
➤ Deep Learning (DL) based network:



General framework of the proposed method

➤ CNN architecture (inspired by EEGNET) :





General structure of our model for data processing in one time-step.

➤ **Baseline study:**

Extracted features

Line Length



Details coefficients for levels 2, 3,
4, 5 using db4 WT



approximate coefficients using db4
WT



Normalized band power of Delta
(1-4 Hz), Theta (4-8 Hz), Alpha
(8-12 Hz), and Beta (12-30 Hz)
band to 1 to 30 Hz

Division of three-second
epochs to three non-
overlapping one-second
epochs

LDA
classifier

Seizure
detection

- **Mozafari et al:**
 - A seizure detection method on the same subset of the TUH dataset
 - consists of clustering, classification, and voting on each cluster
- **Another challenge in our work:** severe imbalance in our classification problem
Our solution: the weighting technique of two-class samples

Classification results of our proposed method (over ten random runs) and the other two methods (Baseline and Mozafari et al.) for seizure detection task

Method	Accuracy (%)	Sensitivity (%)	Specificity (%)	Precision (%)
Mozafari et al.	80.72	80.00	81.08	67.55
Baseline study	71.12	67.10	71.44	67.98
Proposed Method	82.00\pm0.63	85.01\pm0.84	80.22 \pm 0.93	71.69\pm1.01

➤ **Main advantages of our work:**

Automatically extraction of features from raw EEG signals with no pre-defined restrictions



Considering the changes in the pattern of the EEG signals in an epoch



Robustness of our model due to the great performance on a cross-subject scenario

**Thank you,
Any questions?**